396 The Open Orthopaedics Journal, 2016, 10, 396-403

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DOI: 10.2174/1874325001610010396
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DOI: 10.2174/1874325001610010396

RESEARCH ARTICLE

Preoperative Periarticular Knee Bone Mineral Density in Osteoarthritic Patients Undergoing TKA

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Received: February 2, 2016	Revised: June 10, 2016	Accepted: July 15, 2016
Abstract:		

Background:

Preoperative periarticular bone quality is affected by joint loading. The purpose of this study was to determine the periarticular bone mineral density of the knee joint of patients undergoing total knee arthroplasty, and whether the location of the load-bearing axis correlates with the measured bone mineral density.

Materials and Methods:

The bone mineral densities of the medial and lateral femoral condyles and the medial and lateral tibial condyles were analyzed in consecutive 116 osteoarthritic patients (130 knees) by dual energy x-ray absorptiometry.

Results:

The median bone mineral density values in the condyles were 1.138 in femoral medial, 0.767 in femoral lateral, 1.056 in tibial medial, and 0.714 in tibial lateral. The medial condyles showed significantly higher bone mineral densities than the lateral condyles in both the femur and tibia. In addition, the femoral medial showed significantly higher bone mineral density levels than the tibial medial, and the femoral lateral condyle had higher bone mineral density levels than the tibial lateral. The bone mineral density Medial/Lateral ratio was significantly negatively correlated with the location (tibial medial edge 0%, lateral edge 100%) of the load-bearing axis in the femur and tibia.

Conclusion:

Preoperative bone mineral density values may provide against the changes in bone mineral density after total knee arthroplasty by reflecting the correlation with joint loading axis. These results help explain why total knee arthroplasty has such good long-term clinical outcomes with a low frequency of component loosening and periarticular fractures despite a high degree of postoperative bone loss.

Keywords: Dual energy x-ray absorptiometry, Knee, Load-bearing axis, Osteoarthritis, Preoperative bone mineral density, Total knee arthroplasty.

INTRODUCTION

The most common cause of revision arthroplasty is reported to be aseptic loosening [1], which occurs when the periprosthetic bone undergoes resorption. The quality of the osteotomized aspects of the subchondral trabecular bone

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during total knee arthroplasty (TKA) is considered to be the critical biological determinant for the fixation of components in the femur and even more so in the tibia. Measurements of bone mineral density (BMD) using dual energy x-ray absorptiometry (DEXA) allow the noninvasive, *in vivo* evaluation of the mechanical properties of the trabecular bone. Such measurements as well as the architecture of the trabecular patterns, enable the quantitative evaluation of the variations in bone biomechanical characteristics of the knee before a TKA procedure [2, 3].

The loss of peri-prosthetic bone after knee arthroplasty has been shown to adversely influence the migration of implants [3]. Despite this effect, the preoperative bone quality of the knee joint is not routinely assessed during preoperative planning [4]. In addition, although joint loading is related to the periarticular BMD of osteoarthritic knee joints [5, 6], the normal subchondral bone remodeling appears to be deteriorated in the knees of patients with end-stage osteoarthritis (OA) undergoing TKA, as reported with early-stage OA [7]. Therefore, the purpose of the present study was to determine (1) the periarticular BMD of the knee joint of patients undergoing TKA, and (2) whether the location of load-bearing axis (LBA), which is related to joint loading, correlates with the measured BMD. The hypothesis of this study was that the periarticular BMD of the knee is higher on the load-bearing side and correlates with joint loading (i.e. the location of the mechanical axis) in patients undergoing TKA.

MATERIALS AND METHODS

The protocol for this study was approved by the Research Board of Healthcare Corporation Ashinokai, Gyoda, Saitama, Japan, and informed consent was obtained from all patients. One hundred sixteen primary OA patients (130 knees) undergoing TKA were evaluated. The mean age at the time of surgery was 71 years (range: 39-88 years). The pre-operative diagnosis for all patients was OA, and their clinical characteristics are summarized in Table **1**.

Table 1. Patient characteristics.

Parameter	Mean ± S.D.	
Knees / Patients	130 / 116	
Male (# of knees)/ Female (# of knees)	13 (14) / 103 (116)	
Mean age (years); [range]	71 ± 8; [39–88]	
BMI	26 ± 4	
Pre-op. HSS Score	43 ± 11	
Osteoarthritis Grade*	IV: 130	
$LBR < 50\% / 50\% \le LBR$	123 / 7	

Pre-op: pre-operation; S.D.: standard deviation; HSS: Hospital for Special Surgery; LBR: Load Bearing Ratio.

* Osteoarthritis grade was evaluated using the Kellgren and Lawrence radiographic grading scale [8].

Measurement with DEXA

DEXA scans of the periarticular knee joint were acquired using a Lunar Prodigy densitometer (GE Medical Systems, Lunar, Madison, WI, USA) on the day before surgery. A single operator (K.T.) scanned all the knees. For the distal femur and proximal tibia scans, patients were laid in a supine position on a coach, and each knee in turn was positioned within a supportive brace allowing the patella to face upward. Patients who had flexion contracture were measured at their position of maximum knee extension.

The Lunar Prodigy software was used to determine bone mineral content (g) and BMD (g/ cm²) for the proximal medial and lateral regions of interest (ROI) in both the femur and tibia. The BMD values of the femoral and tibial condyles were measured and are referred to as follows: medial femoral condyle: FM; lateral femoral condyle: FL; medial tibial condyle: TM; and lateral tibial condyle: TL. The height of each ROI was 2 cm below the joint line because the osteotomy during TKA surgery is usually performed within a depth of 2 cm. The external border of each ROI extended to the subperiosteal surface of the femur and tibia as determined manually by a single technician (K.T.). The patella served as the inner border for the medial and lateral proximal femoral ROIs, and the intercondylar eminences served as the inner border for the medial and lateral proximal tibial ROIs. In the femoral ROIs, care was taken to avoid including the patella in the measurement. In the lateral ROIs, care was also taken to avoid including the fibula in the medial-to-lateral BMD (BMD M/L) ratio was calculated by dividing the BMD in the medial ROI by the BMD in the lateral ROI in both the femur and tibia. The precision was calculated as the coefficient of variation (% CV) between scan BMD values. The precision of the measurements were 2.6% in FM, 5.5% in FL, 4.3% in TM, and 5.0% in TL.



Fig. (1). Bone mineral density values were measured in the femoral and tibial condyles. FM: medial femoral condyle; FL: lateral femoral condyle; TM: medial tibial condyle; and TL: lateral tibial condyle. The height of each region of interest (ROI) extended to 2 cm below the joint line. The external border of each ROI extended to the subperiosteal surface of the femur and tibia as determined manually. The patella served as the inner border for the medial and lateral proximal femoral ROIs, and the intercondylar eminences served as the inner border for the medial and lateral proximal femoral ROIs, care was taken to avoid including the patella in the measurements. In the lateral ROIs, care was also taken to avoid including the fibula in the measurements.

Definition of the Load-bearing Mechanical Axis

Full-length load-bearing anteroposterior computed radiography (CR) images of the lower extremities were obtained before TKA. The mechanical axis was defined by a line connecting the center of the femoral head and the center of the ankle [9]. The load-bearing ratio (LBR) was calculated by measuring the distance from the medial edge of the proximal tibia to the point where the mechanical axis intersected the proximal tibia (tibial plateau level), and then dividing that measurement by the entire width of the proximal tibia and multiplying the ratio by 100%. Therefore, the percentage value can be negative (-) when the axis intersected more medially than the medial edge of the proximal tibia, and more than 100% when it intersected more laterally than the lateral edge.

Statistical Analysis

The BMD values in each condyle were compared using the Friedman test and Scheffé's multiple comparison test. Spearman's correlation of rank coefficients was used to evaluate the relationships between the BMD values in each condyle and between the BMD M/L ratio and the mechanical load-bearing axis. The strength of the correlation of the rank coefficients was defined as strong for values of 0.7-1.0; moderate for 0.4-0.7; and weak for 0.2-0.4. The BMD value is expressed using the median (25^{th} percentile, 75^{th} percentile). Statistical analyses were performed using SPSS software (ver. 14.0 J; SPSS, Tokyo, Japan). In all tests, *p* values less than 0.05 were considered statistically significant.

RESULTS

The median BMD values in the condyles were 1.138 (0.976, 1.287) in FM, 0.767 (0.647, 0.916) in FL, 1.056 (0.894, 1.216) in TM, and 0.714 (0.600, 0.843) in TL (Table 2). The medial condyles showed significantly higher values than the lateral condyles in both the femur and tibia (FM vs. FL: p<0.001; TM vs. TL: p<0.001). In addition, we found that the FM showed significantly higher BMD levels than the TM (p=0.009), and the FL had higher BMD levels than the TL (p=0.004).

	FM	FL	ТМ	TL	M/L Femur	M/L Tibia
Median	1.138	0.767	1.056	0.714	1.469	1.481
25 percentile	0.976	0.647	0.894	0.600	1.269	1.326
75 percentile	1.287	0.916	1.216	0.843	1.754	1.683

BMD: bone mineral density; FM: medial femoral condyle; FL: lateral femoral condyle; TM: medial tibial condyle; TL: lateral tibial condyle; M/L: Medial BMD / Lateral BMD ratio.

Strong correlations were found between the BMD levels in the FM and TM (p<0.0001, r=0.842), and between the FL and TL (p<0.0001, r=0.847). Additionally, a weak correlation was found between the BMD levels in the FM and FL (p<0.0001, r=0.364), and a moderate correlation was found between the TM and TL (p<0.0001, r=0.490).

In 123 out of the 130 knees (95%), the LBA passed through the medial side at the tibial plateau level (Tables 1 and 3). There were moderate, negative correlations between the BMD M/L ratio and LBR in the femur (p<0.0001, r=-0.408) and tibia (p<0.0001, r=-0.427) (Fig. 2a and b).

Table 3. Distribution of the preoperative load-bearing ratio at the tibial plateau level

LBR	LBR < 0	0 ≤LBR<50	50≤LBR<100	100≤ LBR
Number of knees	84	39	5	2

LBR: load-bearing ratio

DISCUSSION

Three important findings in the present study should be highlighted. First, the BMD levels were significantly higher in the medial than lateral condyles of the femoral and tibial bones. The main reason for this might be that the LBA of 95% of the knees studied here passed through the condyles at less than 50% of the tibial plateau level. Because OA usually develops first on the medial condyle, progressing to the lateral condyle as the condition worsens, our data support the conclusions of previous studies that reported a positive correlation between OA grade and BMD values [6, 10 - 13]. Second, the BMD values of the femoral sides were higher than those of the tibial sides. Because the femur is characterized by a convex geometry and the tibia by a concave geometry in this study, there may be anatomy- and geometry-specific bone characteristics that account for the differences in the BMD values between the femur and tibia. Third, the BMD M/L ratios in each femur and tibia in end-stage OA before TKA surgery were significantly correlated with the location of the LBA, confirming a previous report in osteoarthritic knees in various stage OA [5, 6].





Fig. (2). The bone mineral density medial / lateral ratio and load-bearing ratio were moderately negatively correlated in both the femur (A) and tibia (B).

The preoperative BMD values from patients undergoing TKA surgery were previously reported at the proximal femur and lumbar spine [4, 14 - 16]. In some cases, the periarticular BMD of the knee joint was evaluated on the femoral side [14, 17], the tibial side [15, 18 - 20], or on both sides [21 - 23]. The preoperative BMD values of the femur and tibia measured in the present study were within the range of previously reported values [12, 14, 15, 17 - 19, 22, 23] in the femur (0.512-1.70) and tibia (0.500-1.366). In addition, the BMD M/L ratio was also within the range of previously reported values [5, 6, 10] for osteoarthritic knee joints. Because there were significant correlations of the preoperative BMDs both between the femur and tibia for the medial and lateral compartments, and between the medial and lateral compartments for the femur and tibia, similar subchondral bone remodeling under various load-bearing conditions may occur in each compartment of the femur and tibia in each patient. Akamatsu *et al.* [10] also showed a significant positive correlation between the femoral and tibial condyles in 2 groups according to joint space narrowing in the following parameters: medial condyle BMDs, lateral condyle BMDs, and medial *versus* lateral condyle BMD ratios, supporting our results.

After TKA surgery, the postoperative BMD values are known to decrease, which is believed to affect prosthetic fixation. Such decreases in BMD were reported in the femur [17, 24], tibia [25 - 27], and in both sides [21, 22, 28]. Abu-Rajab *et al.* [28] demonstrated less reduction in bone density around the tibial component than around the femoral component. Levitz *et al.* [25] reported that eight years after TKA, there was a 36.4% decrease in tibial BMD, on average. Additionally, Petersen *et al.* [24] reported that BMD decreased by an average of 36% behind the anterior flange of the femoral prosthesis *after only 2 years.*

Despite of such large and faster decreases in BMD in the femur than in the tibia, periprosthetic fractures, such as supracondylar fractures of the femur, following TKA are not common. The higher preoperative BMD values in the femur than in the tibia indicated by the present study might play an important role in maintaining enough subchondral bone density to prevent component loosening and fractures around the component despite the rapid bone loss in the femur. We believe it is reasonable to think that the BMDs in the femur and tibia may approach similar values after TKA surgery.

Soininvaara *et al.* [29] reported similar medial and lateral BMD values in knees corrected for varus and valgus deformities due to bone remodeling after alignment correction through TKA. Additionally, Petersen *et al.* [20] reported that for tibial condyles in which the change in knee alignment indicated that the load was reduced postoperatively, a fast

bone loss of 7-20% was seen during the first 6 months after surgery. A small, but significant increase in BMD of 2-7% was seen in tibial condyles in which the experienced load was increased after uncemented TKA. These studies, including our own, suggest that the bones become equally strong in both compartments of the metaphysis of the femur and tibia after TKA surgery. Such adaptation of the subchondral bone beneath each component may prevent clinical failures induced by the collapse of the trabecular bone. Soininvaara *et al.* [29] also concluded that the resultant equilibrium in bone density and strength potentially helps increase the longevity of TKA by creating more optimal loading conditions. In addition, Petersen *et al.* [20] concluded that a portion of the bone loss after TKA may represent a return to the normal, relatively high density arthritic bone that helps to make the long-term outcomes after TKA satisfactory, with a low revision rate and fractures of the proximal tibia rarely occurring.

Finally, considering that 123 out of the 130 knees (95%) showed less than 50% of the LBR passing through the tibial plateau level in this study, it is reasonable that the medial condyles of the femur and tibia had significantly higher BMD levels than the lateral condyles because joint loading may correlate with the periarticular BMD, as previously reported in both mild and severe osteoarthritic knee joints [5, 6]. The present study revealed that joint loading was correlated with the periarticular BMD of the knee joints of end-stage OA patients undergoing TKA. In addition, there was a significant correlation between the BMD M/L ratio in the femur and tibia and the LBR. Based on this data, orthopedic surgeons should consider, while performing TKA surgeries, that large differences in the load-bearing mechanical axis in the knee joint may indicate large differences in BMD values between the medial and lateral condyles, if the BMDs were not measured during pre-operative planning.

The LBR was positively correlated with the BMD M/L ratio of the femur and tibia before TKA surgery. Additionally, higher preoperative BMD values were found in the load-bearing side (*i.e.* the medial side in this study), while the femur showed larger and faster decreases in BMD than the unloaded side (*i.e.* the lateral side) and the tibia showed less loss. The distribution of preoperative BMD values reported in the present study may provide against the loss of BMD following TKA.

Several limitations of this study should be discussed. First, the results cannot be generalized to all osteoarthritis patients. Based on the results of LBR that over 95% of the patients showed less than 50%, most of them were the predominance of the varus knee with a few valgus knee. Second, because the height of each ROI reached to 2 cm below the joint line, variations in the degree of deformity of the condyles and in the level of the femoral and tibial scans at the time of measurement may have been sources of bias in this study. Third, the LBA was evaluated only with the coronal plane because of the study protocol. A three-dimensional approach using the load-bearing mechanical axes in both the anteroposterior and mediolateral directions would be more accurate for identifying the load distribution on the knee joint compared to a 2-dimensional approach using either individual axis [30]. Finally, because the evaluation of the BMD in the femur was performed 2 cm below the joint line in the coronal plane, no follow-up study can be performed to compare the pre- and post-operative BMDs, as is reported by most previous studies that were performed in the sagittal plane [14, 17, 21, 24, 28].

Despite these limitations, the strengths of the study include that we showed the preoperative periarticular BMD of knee joints including the osteotomized level, which is often considered to be the critical biological determinant for the fixation of components in the femur and tibia.

CONCLUSION

In conclusion, the results of the current study help explain why TKA has such good long-term clinical outcomes with a low frequency of component loosening and periarticular fractures despite a high degree of postoperative bone loss. The evaluation of the preoperative periarticular bone quality might be recommended during pre-operative planning before TKA routinely, since the quality of the osteotomized aspects of the subchondral trabecular bone during TKA is considered to be the critical biological determinant for the fixation of components in the femur and even more so in the tibia.

CONFLICT OF INTEREST

The authors confirm that this article content has no conflict of interest.

ACKNOWLEDGEMENTS

This work was performed at Ishii Orthopaedic and Rehabilitation Clinic, Gyoda, Saitama, Japan.

REFERENCES

- Sharkey PF, Lichstein PM, Shen C, Tokarski AT, Parvizi J. Why are total knee arthroplasties failing today--has anything changed after 10 years? J Arthroplasty 2014; 29(9): 1774-8.
 [http://dx.doi.org/10.1016/j.arth.2013.07.024] [PMID: 25007726]
- [2] Hvid I, Hasling C, Hansen SL, Hansen HH. Dual-photon absorptiometry of the proximal tibia. Arch Orthop Trauma Surg 1987; 106(5): 314-8.

[http://dx.doi.org/10.1007/BF00454340] [PMID: 3632318]

- [3] Petersen MM, Jensen NC, Gehrchen PM, Nielsen PK, Nielsen PT. The relation between trabecular bone strength and bone mineral density assessed by dual photon and dual energy X-ray absorptiometry in the proximal tibia. Calcif Tissue Int 1996; 59(4): 311-4. [http://dx.doi.org/10.1007/s002239900131] [PMID: 8781060]
- [4] James SJ, Mirza SB, Culliford DJ, Taylor PA, Carr AJ, Arden NK. Baseline bone mineral density and boneturnover in pre-operative hip and knee arthroplasty patients. Bone Joint Res 2014; 3(1): 14-9. [http://dx.doi.org/10.1302/2046-3758.31.2000218] [PMID: 24443424]
- [5] Thorp LE, Wimmer MA, Block JA, et al. Bone mineral density in the proximal tibia varies as a function of static alignment and knee adduction angular momentum in individuals with medial knee osteoarthritis. Bone 2006; 39(5): 1116-22. [http://dx.doi.org/10.1016/j.bone.2006.05.001] [PMID: 16782419]
- [6] Wada M, Maezawa Y, Baba H, Shimada S, Sasaki S, Nose Y. Relationships among bone mineral densities, static alignment and dynamic load in patients with medial compartment knee osteoarthritis. Rheumatology (Oxford) 2001; 40(5): 499-505. [http://dx.doi.org/10.1093/rheumatology/40.5.499] [PMID: 11371657]
- [7] Ding M, Odgaard A, Hvid I. Changes in the three-dimensional microstructure of human tibial cancellous bone in early osteoarthritis. J Bone Joint Surg Br 2003; 85(6): 906-12.
 [PMID: 12931817]
- [8] Kellgren JH, Lawrence JS. Radiological assessment of osteo-arthrosis. Ann Rheum Dis 1957; 16(4): 494-502. [http://dx.doi.org/10.1136/ard.16.4.494] [PMID: 13498604]
- [9] Ishii Y, Ohmori G, Bechtold JE, Gustilo RB. Extramedullary *versus* intramedullary alignment guides in total knee arthroplasty. Clin Orthop Relat Res 1995; (318): 167-75.
 [PMID: 7671512]
- [10] Akamatsu Y, Mitsugi N, Taki N, Kobayashi H, Saito T. Medial versus lateral condyle bone mineral density ratios in a cross-sectional study: a potential marker for medial knee osteoarthritis severity. Arthritis Care Res (Hoboken) 2012; 64(7): 1036-45. [PMID: 22371312]
- [11] Clarke S, Wakeley C, Duddy J, et al. Dual-energy X-ray absorptiometry applied to the assessment of tibial subchondral bone mineral density in osteoarthritis of the knee. Skeletal Radiol 2004; 33(10): 588-95. [http://dx.doi.org/10.1007/s00256-004-0790-x] [PMID: 15221213]
- [12] Hulet C, Sabatier JP, Souquet D, Locker B, Marcelli C, Vielpeau C. Distribution of bone mineral density at the proximal tibia in knee osteoarthritis. Calcif Tissue Int 2002; 71(4): 315-22. [http://dx.doi.org/10.1007/s00223-001-2112-9] [PMID: 12202957]
- [13] Lo GH, Zhang Y, McLennan C, et al. The ratio of medial to lateral tibial plateau bone mineral density and compartment-specific tibiofemoral osteoarthritis. Osteoarthritis Cartilage 2006; 14(10): 984-90. [http://dx.doi.org/10.1016/j.joca.2006.04.010] [PMID: 16765066]
- [14] Ishii Y, Noguchi H, Takeda M, Sato J, Ezawa N, Toyabe S. Changes of three-dimensional load bearing axis in lower extremity between before and after total knee arthroplasty --Comparison between meniscal bearing and rotating platform design. J Arthroplasty 2012; 27(6): 1203-9.
 [http://dx.doi.org/10.1016/j.arth.2011.12.013] [PMID: 22305436]
- [15] Abu-Rajab RB, Watson WS, Walker B, Roberts J, Gallacher SJ, Meek RM. Peri-prosthetic bone mineral density after total knee arthroplasty. Cemented versus cementless fixation. J Bone Joint Surg Br 2006; 88(5): 606-13. [http://dx.doi.org/10.1302/0301-620X.88B5.16893] [PMID: 16645105]
- [16] Järvenpä J, Soininvaara T, Kettunen J, Miettinen H, Kröger H. Changes in bone mineral density of the distal femur after total knee arthroplasty: a 7-year DEXA follow-up comparing results between obese and nonobese patients. Knee 2014; 21(1): 232-5. [http://dx.doi.org/10.1016/j.knee.2013.03.004] [PMID: 23566738]
- [17] Minoda Y, Ikebuchi M, Kobayashi A, Iwaki H, Inori F, Nakamura H. A cemented mobile-bearing total knee replacement prevents periprosthetic loss of bone mineral density around the femoral component: a matched cohort study. J Bone Joint Surg Br 2010; 92(6): 794-8. [http://dx.doi.org/10.1302/0301-620X.92B6.23159] [PMID: 20513875]
- Petersen MM, Olsen C, Lauritzen JB, Lund B. Changes in bone mineral density of the distal femur following uncemented total knee arthroplasty. J Arthroplasty 1995; 10(1): 7-11.
 [http://dx.doi.org/10.1016/S0883-5403(06)80058-6] [PMID: 7730833]
- [19] Wang CJ, Wang JW, Weng LH, Hsu CC, Huang CC, Chen HS. The effect of alendronate on bone mineral density in the distal part of the femur and proximal part of the tibia after total knee arthroplasty. J Bone Joint Surg Am 2003; 85-A(11): 2121-6.

[PMID: 14630840]

- [20] Minoda Y, Kobayashi A, Iwaki H, Ikebuchi M, Inori F, Takaoka K. Comparison of bone mineral density between porous tantalum and cemented tibial total knee arthroplasty components. J Bone Joint Surg Am 2010; 92(3): 700-6. [http://dx.doi.org/10.2106/JBJS.H.01349] [PMID: 20194329]
- [21] Soininvaara TA, Miettinen HJ, Jurvelin JS, Alhava EM, Kröger HP. Bone mineral density in the proximal femur and contralateral knee after total knee arthroplasty. J Clin Densitom 2004; 7(4): 424-31. [http://dx.doi.org/10.1385/JCD:7:4:424] [PMID: 15618604]
- [22] Harrison AK, Gioe TJ, Simonelli C, Tatman PJ, Schoeller MC. Do porous tantalum implants help preserve bone?: evaluation of tibial bone density surrounding tantalum tibial implants in TKA. Clin Orthop Relat Res 2010; 468(10): 2739-45. [http://dx.doi.org/10.1007/s11999-009-1222-y] [PMID: 20066524]
- [23] Li MG, Nilsson KG. The effect of the preoperative bone quality on the fixation of the tibial component in total knee arthroplasty. J Arthroplasty 2000; 15(6): 744-53. [http://dx.doi.org/10.1054/arth.2000.6617] [PMID: 11021450]
- [24] Petersen MM, Nielsen PT, Lauritzen JB, Lund B. Changes in bone mineral density of the proximal tibia after uncemented total knee arthroplasty. A 3-year follow-up of 25 knees. Acta Orthop Scand 1995; 66(6): 513-6. [http://dx.doi.org/10.3109/17453679509002305] [PMID: 8553818]
- [25] Gazdzik TS, Gajda T, Kaleta M. Bone mineral density changes after total knee arthroplasty: one-year follow-up. J Clin Densitom 2008; 11(3): 345-50.

[http://dx.doi.org/10.1016/j.jocd.2008.04.007] [PMID: 18619880]

- [26] Wang CJ, Wang JW, Ko JY, Weng LH, Huang CC. Three-year changes in bone mineral density around the knee after a six-month course of oral alendronate following total knee arthroplasty. A prospective, randomized study. J Bone Joint Surg Am 2006; 88(2): 267-72. [http://dx.doi.org/10.2106/JBJS.E.00051] [PMID: 16452736]
- [27] Levitz CL, Lotke PA, Karp JS. Long-term changes in bone mineral density following total knee replacement. Clin Orthop Relat Res 1995; (321): 68-72.
 [PMID: 7497687]
- [28] Li MG, Nilsson KG. No relationship between postoperative changes in bone density at the proximal tibia and the migration of the tibial component 2 years after total knee arthroplasty. J Arthroplasty 2001; 16(7): 893-900. [http://dx.doi.org/10.1054/arth.2001.24376] [PMID: 11607906]
- [29] Saari T, Uvehammer J, Carlsson L, Regnér L, Kärrholm J. Joint area constraint had no influence on bone loss in proximal tibia 5 years after total knee replacement. J Orthop Res 2007; 25(6): 798-803. [http://dx.doi.org/10.1002/jor.20358] [PMID: 17318893]
- [30] Soininvaara TA, Miettinen HJ, Jurvelin JS, Suomalainen OT, Alhava EM, Kröger HP. Periprosthetic tibial bone mineral density changes after total knee arthroplasty: one-year follow-up study of 69 patients. Acta Orthop Scand 2004; 75(5): 600-5. [http://dx.doi.org/10.1080/00016470410001493] [PMID: 15513494]

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